



MRgRT-DOS
Metrology



CCRI webinar (September 12, 2023)

Small field dosimetry for MRgRT: Performance of scintillators in presence of magnetic fields

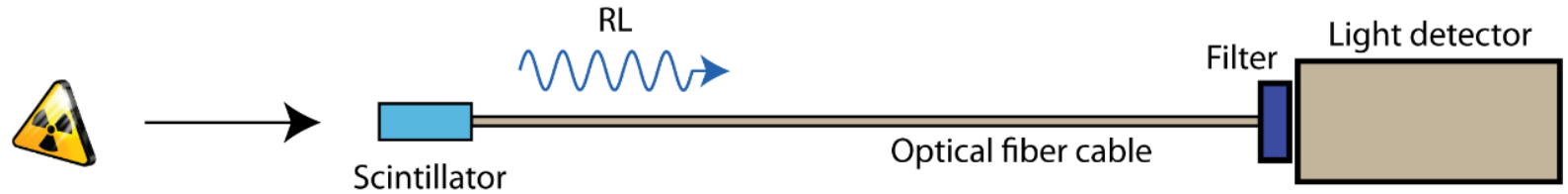
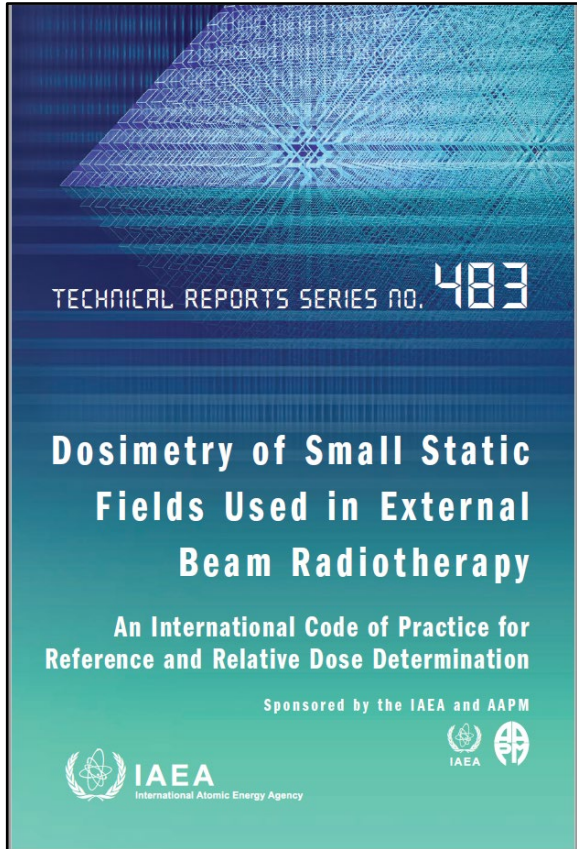
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TRS-483



Main driver for scintillators:

Essentially perturbation-free

Time-resolved

Main application:

Short-term, relative dosimetry

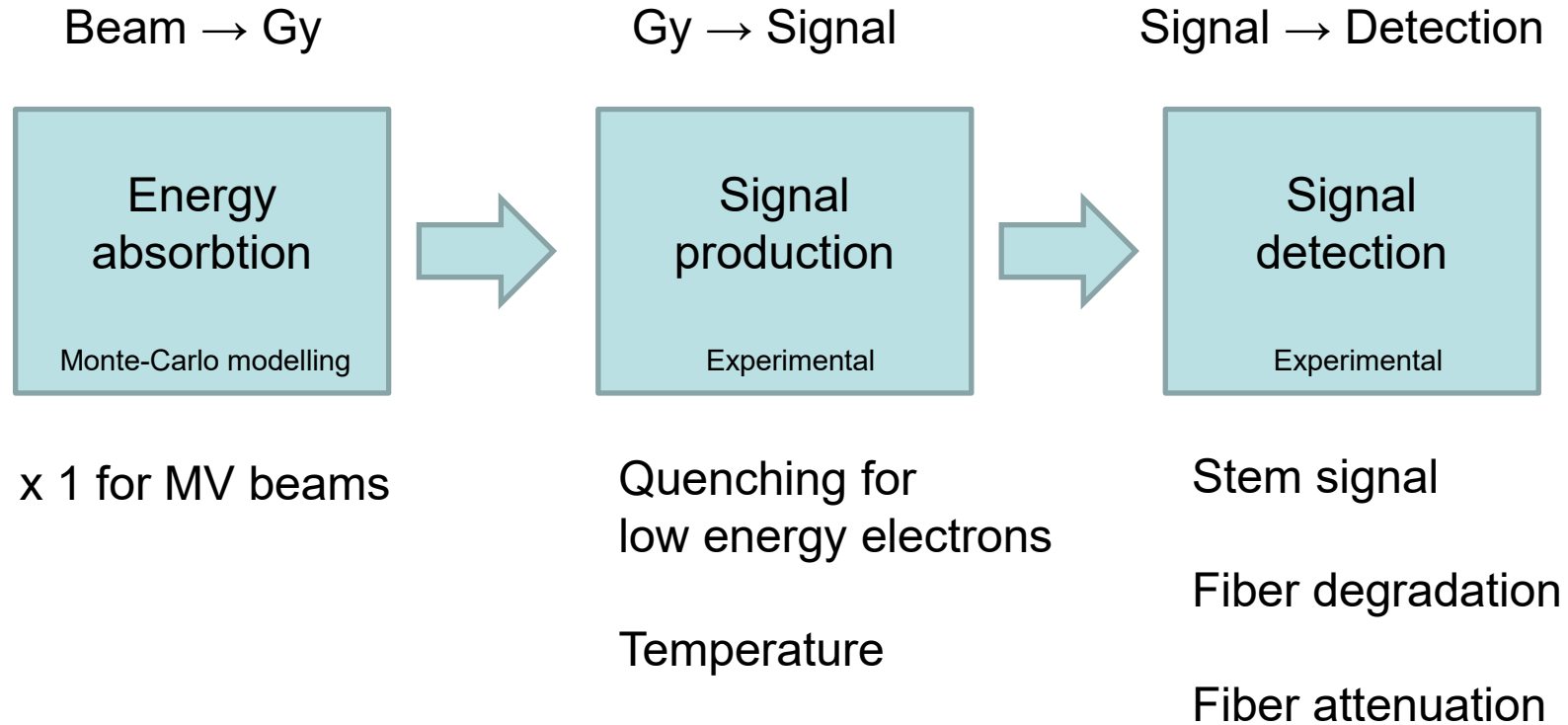
TABLE 24. FIELD OUTPUT CORRECTION FACTORS $k_{clin}^{f_{clin} / f_{msr}}$ FOR TOMOTHERAPY MACHINES, AS A FUNCTION OF THE EQUIVALENT SQUARE FIELD SIZE (cont.)

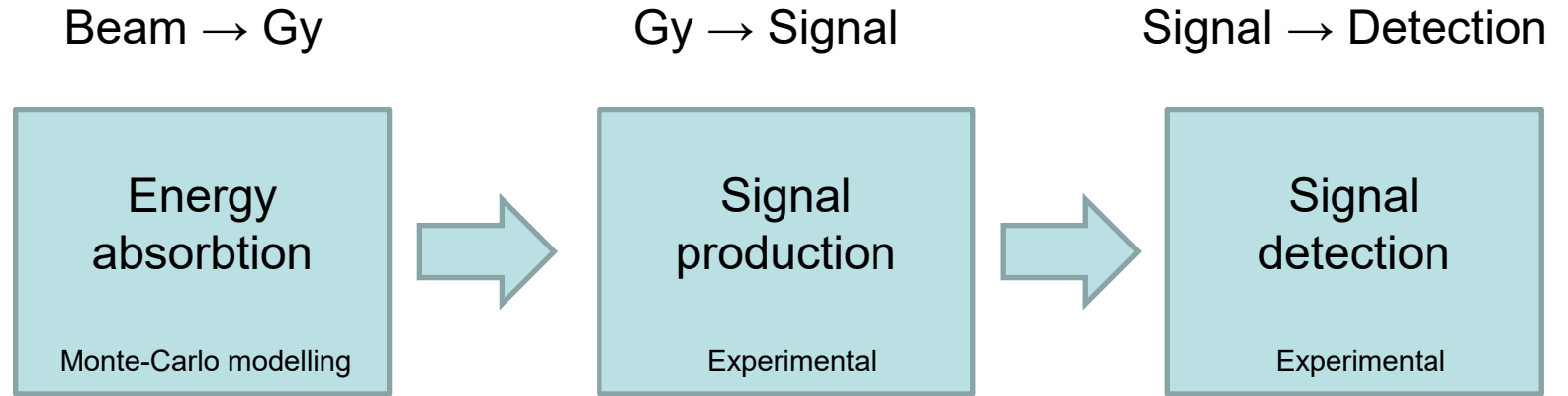
Detector	Equivalent square field size, S_{clin} (cm)												
	5.0	4.0	3.5	3.0	2.5	2.0	1.5	1.2	1.0	0.8	0.6	0.5	0.4
PTW 31018 liquid ion chamber	0.997	0.995	0.994	0.994	0.993	0.992	0.991	0.991	0.992	0.994	1.003	1.015	1.038
Sun Nuclear EDGE Detector	1.000	1.000	1.000	0.999	0.998	0.994	0.986	0.976	0.966	0.951	—	—	—
Standard Imaging W1 plastic scintillator	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000

Note: The msr field is 5 cm × 10 cm and the reference depth is 10 cm.

Multiply by 1.000 !

The three-step dosimetry model for organic plastic scintillator detectors





x 1 for MV beams

Quenching for low energy electrons

Temperature

S. Buranurak et al. (2013)

Wootton & Bedar (2013)

Stem signal

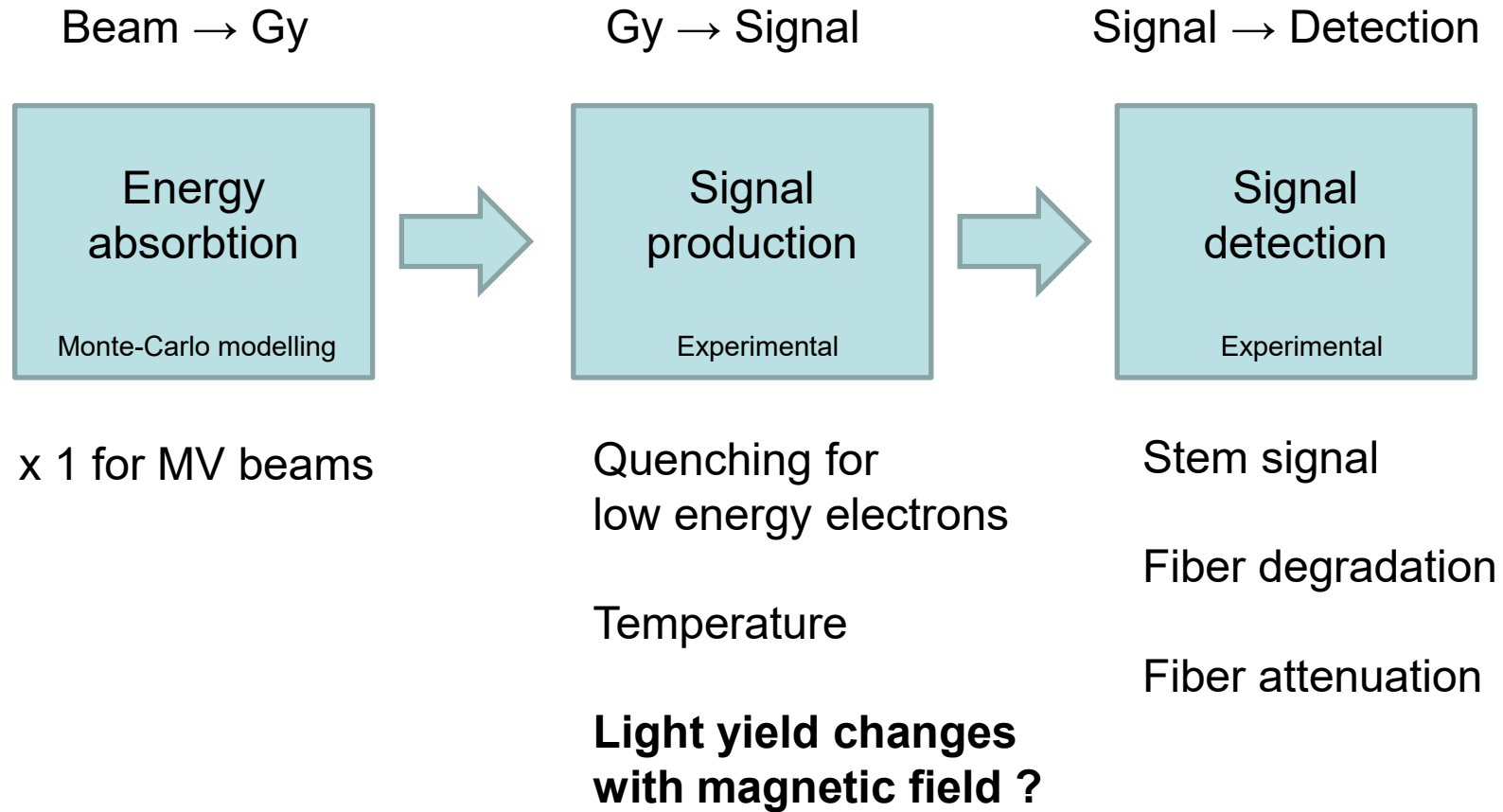
Fiber degradation

Fiber attenuation

Grichar V. Santurio & C.E. Andersen: *Quantifying the ionization quenching effect in organic plastic scintillators used in MV photon dosimetry*. Rad. Meas. 2019.

Effect on field output factor meas.: (0.6 +/- 0.2)% k = 1

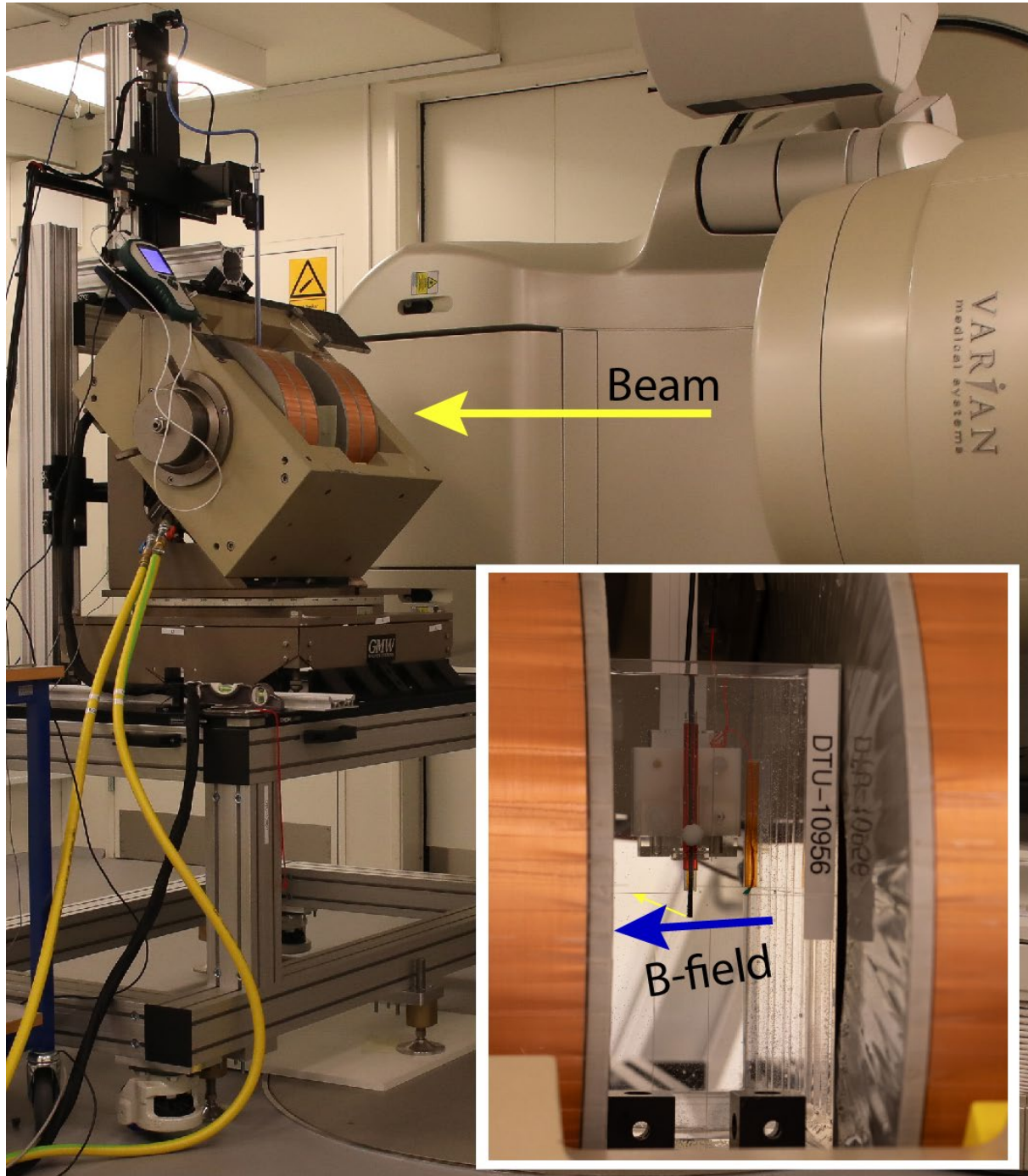
Effect on k_Q measurements: (2.0 +/- 0.4)%



S. Stefanowicz et al.: *Dosimetry in clinical static magnetic fields using plastic scintillation detectors.*
Rad. Meas. (2013).

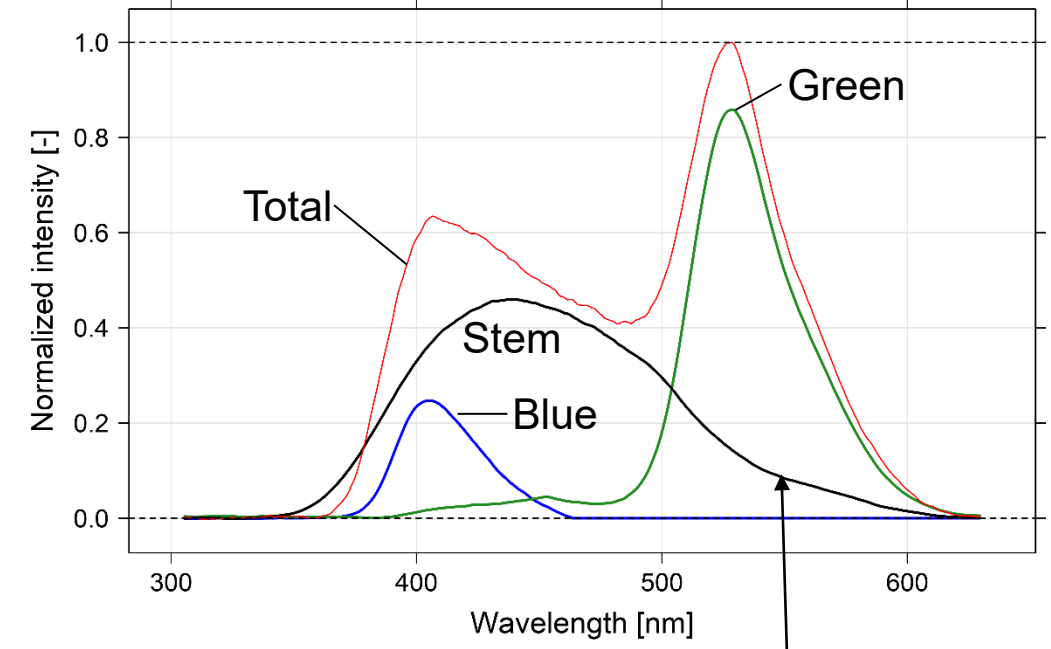
E. Simiele et al.: *Spectral characterization of plastic scintillation detector response as a function of magnetic field strength.*
Phys. Med. Biol. (2018).

F. Therriault-Proulx et al.: *Effect of magnetic field strength on plastic scintillation detector response.*
Rad. Meas. (2018).

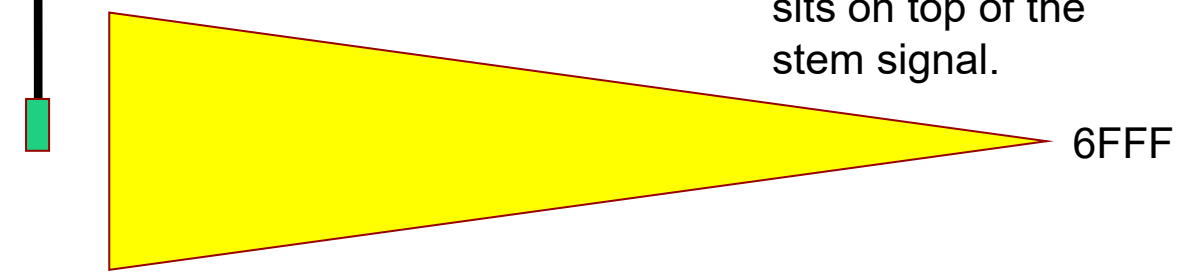


Fiber cable + 2 mm BCF-60

Monochromator spectrum at B = 0 T



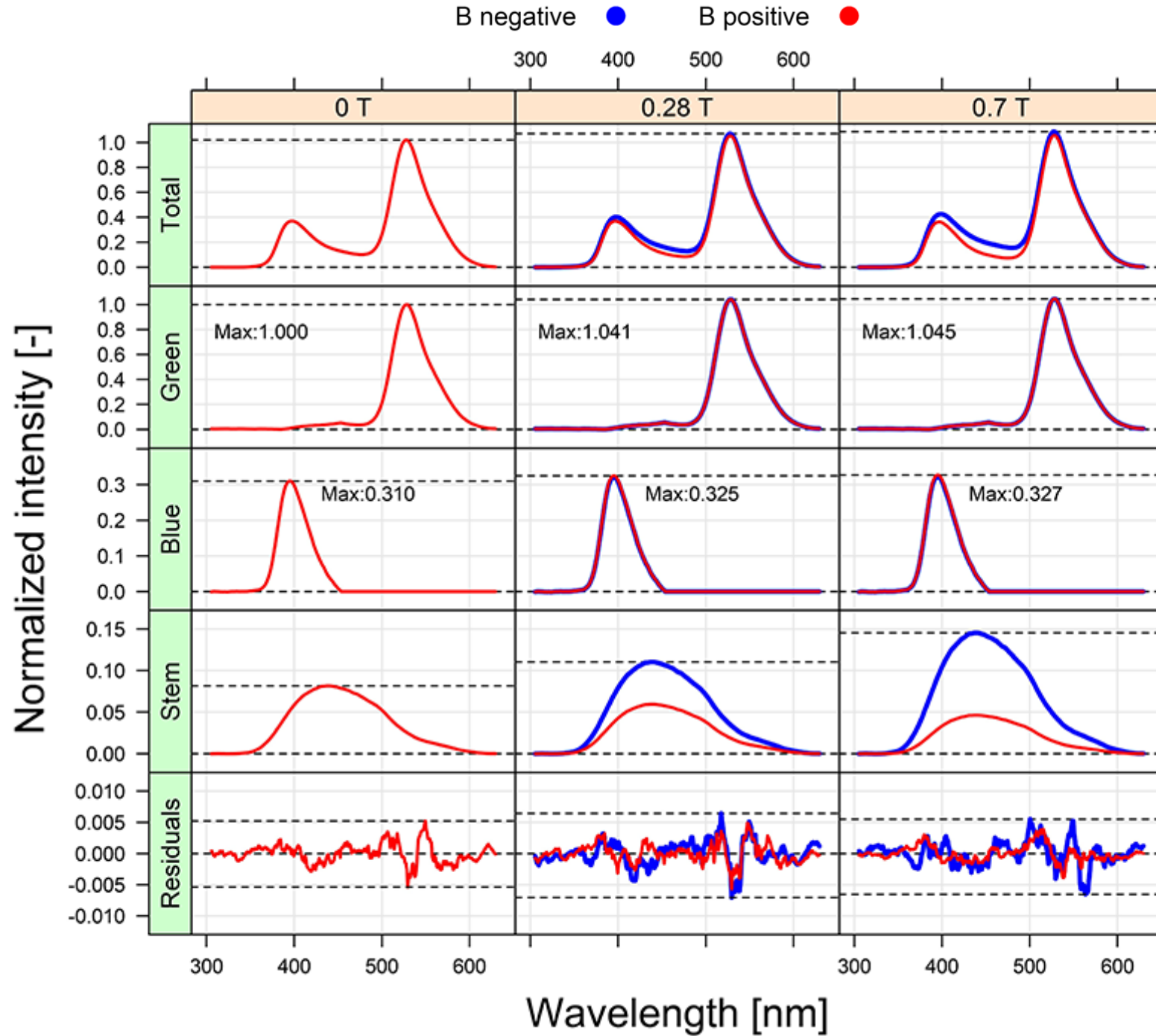
Note how the "green" sits on top of the stem signal.



Extended distance to linac source: 180 cm

Transverse magnetic field

Lorentz force on electrons mainly down (B pos.) or up (B neg.)



Measurements in electromagnet

Field size :
Nominal 50 mm x 50 mm

Beam:
10FFF

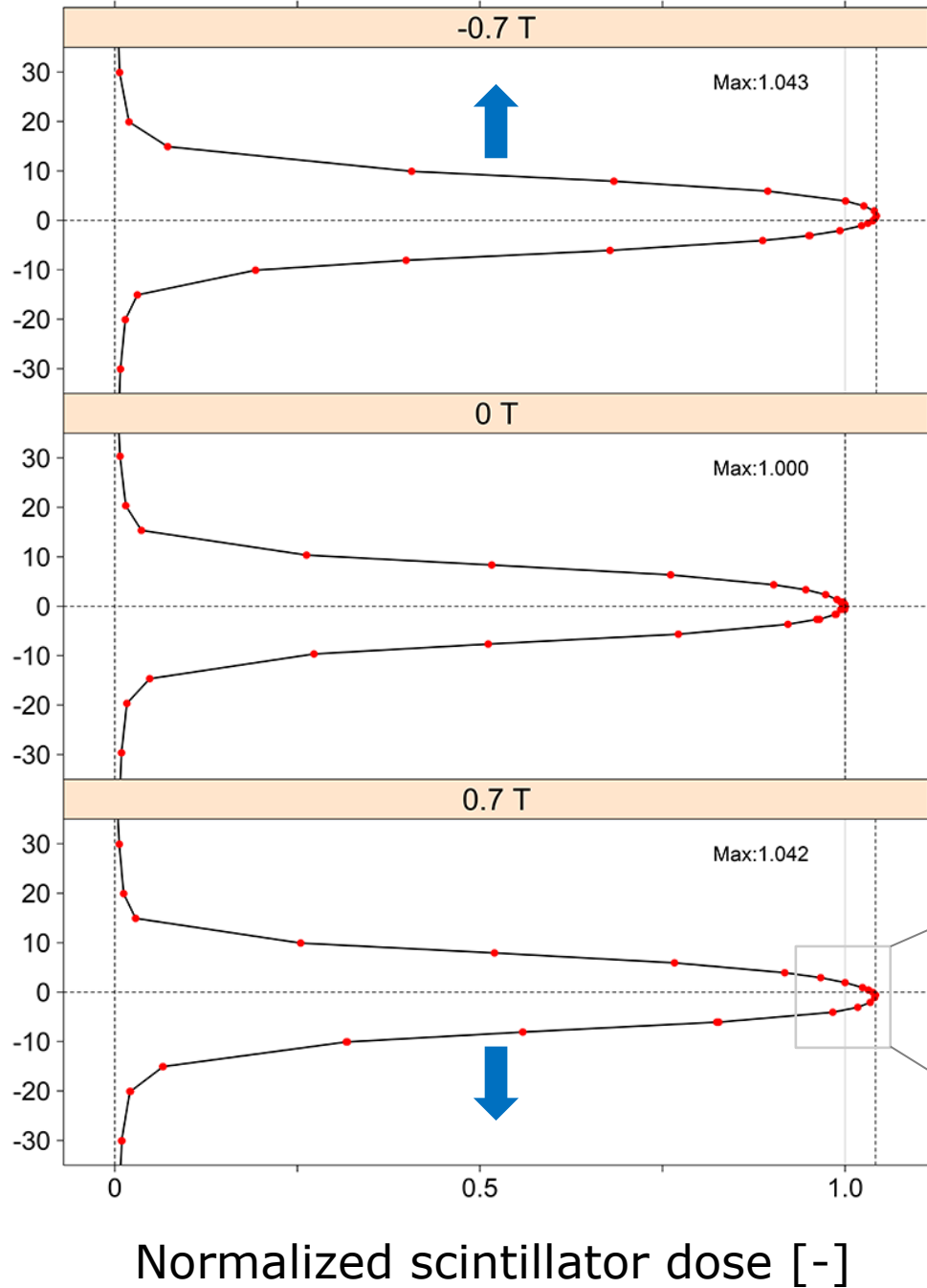
Scintillator:
10 mm BCF-60

Orientation:
Perpendicular to beam

Full separation of green and stem.

Clear effect of magnetic field on scintillator light yield.

Vertical coordinate [mm]



Vertical scans in electromagnet

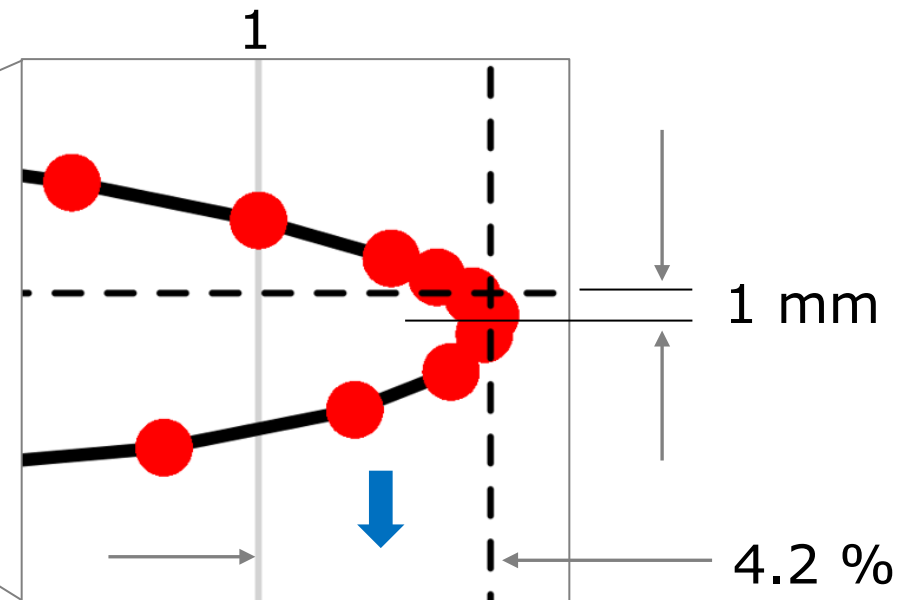
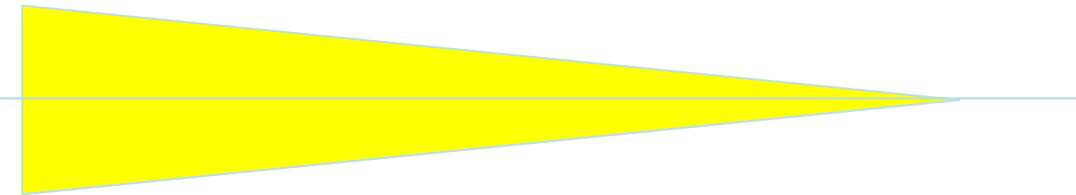
Field size : Nominal 10 mm x 10 mm

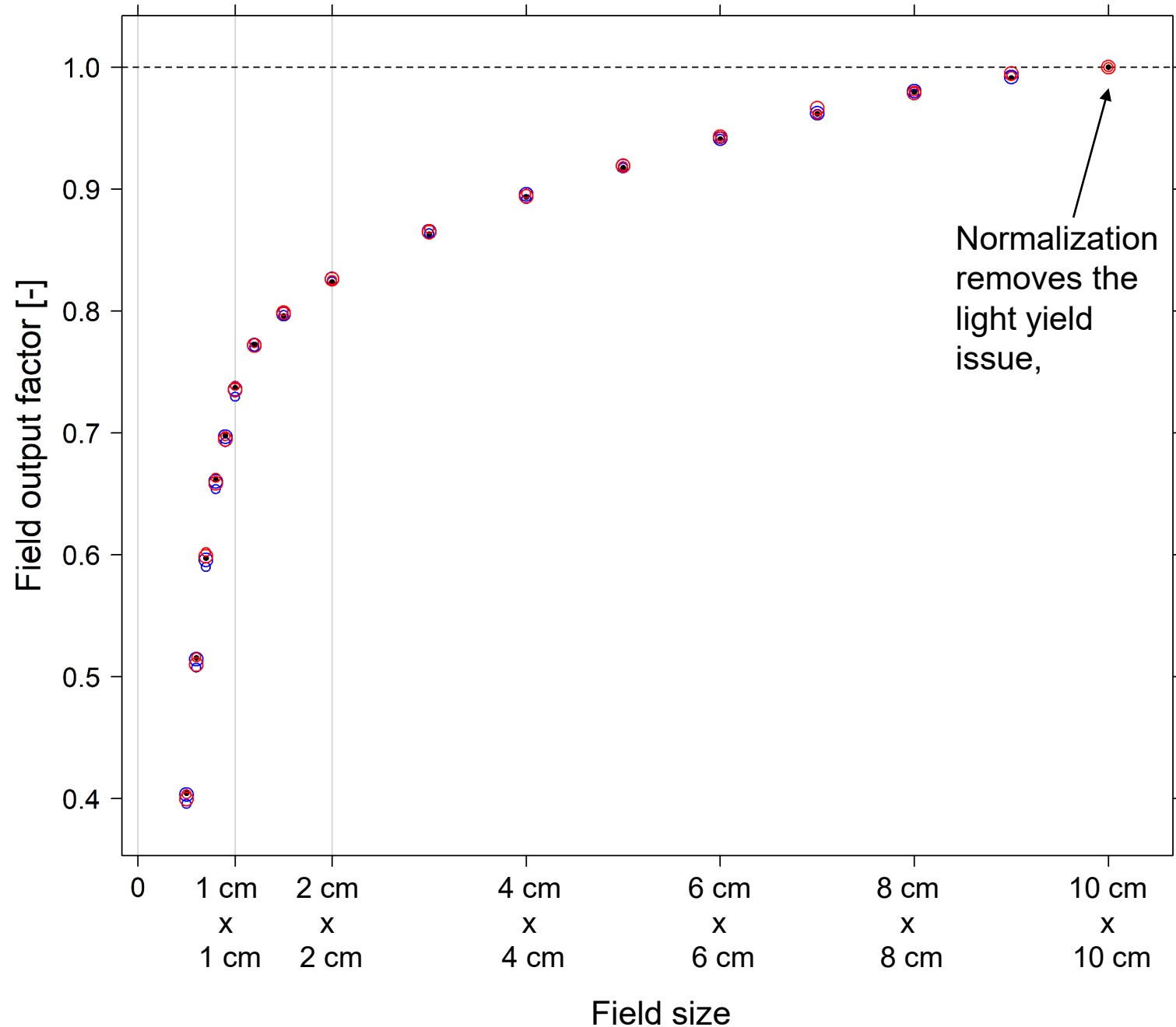
Beam: 6FFF

Scintillator: 2 mm BCF-60

Orientation: Perpendicular to beam

Stem removal: Two-channel chromatic (ME40)





Scintillator based field-output factor measurements in electromagnet at dose maximum

6FFF beam

There is no significant change in field-output factors when measured at the maximum dose point.

The scintillator measurements show that the main effect of the magnetic field is that the maximum dose point is moved.

Normalization removes the light yield issue,

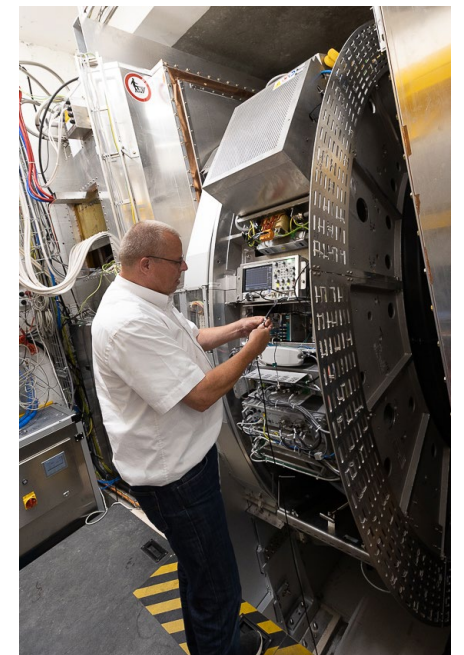
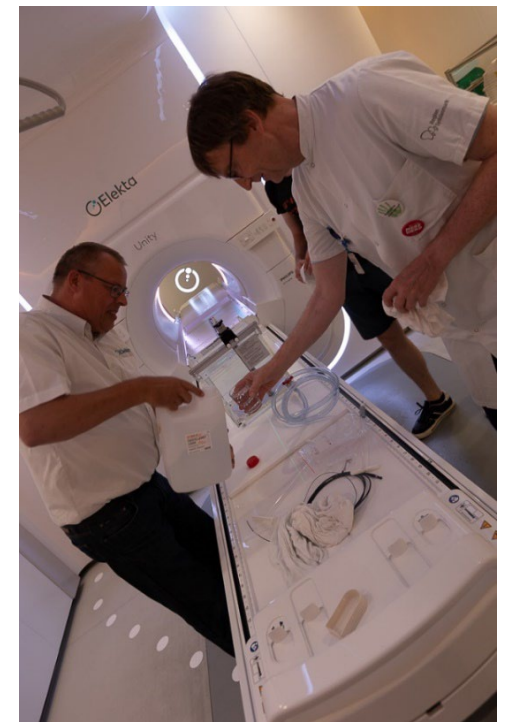
Scintillator-based field output factor measurements in MR linacs at five hospitals

University Hospitals: Heidelberg, Herlev, Odense, Rigshospitalet, and Zürich.

Uncertainty budget for field-output factor measurement in MR linac at 0.5 cm x 0.5 cm relative to 10 cm x 10 cm.

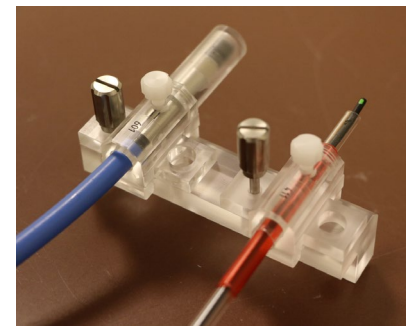
	Type A	Type B
Reproducibility*	0.1 %	
Stem signal correction		0.48 %
Attenuation correction		0.10 %
Position		0.91 %
Calibration		0.07 %
Ionization quenching		0.61 %
Combined uncertainty (k=1)	1.2 %	

*MR-linac dependent



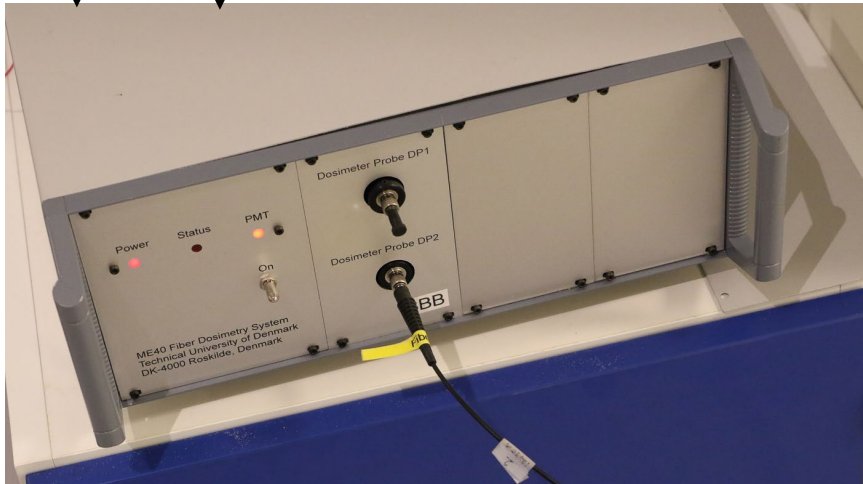


Dose-per-pulse measurements ME40 scintillator system (DTU)

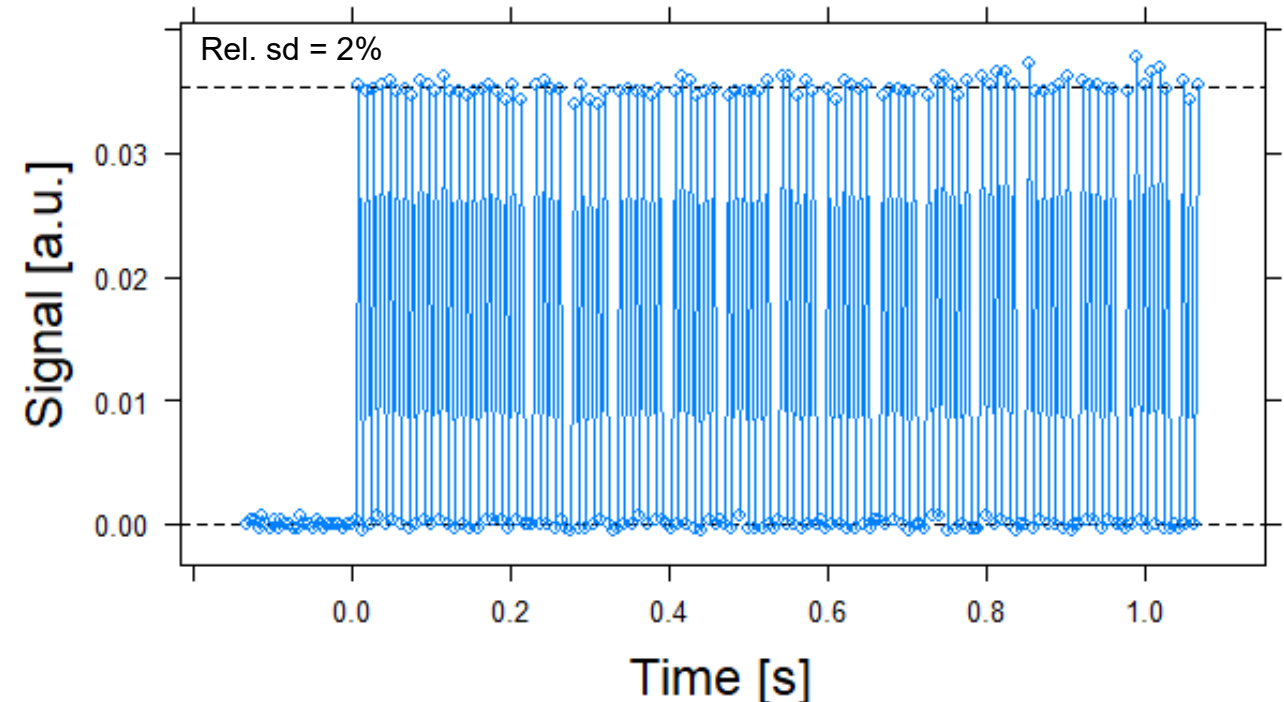


Scintillator
ø1 mm

Sync
Gun pulse



DPP green & blue ch.



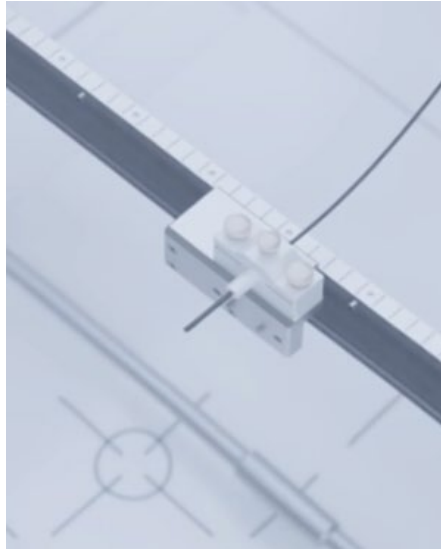
Where we use the high time resolution:

Klavsen et al.: *Time-resolved plastic scintillator dosimetry in MR linear accelerators without image distortion.* *Rad. Meas.* (2022).

Klavsen et al.: *Accumulated dose implications from systematic dose-rate transients in gated treatments with Viewray MRIdian accelerators.* *Biomed. Phys. Eng. Express* (2023).

Exradin® W2 Scintillator

Measurement
without
perturbation



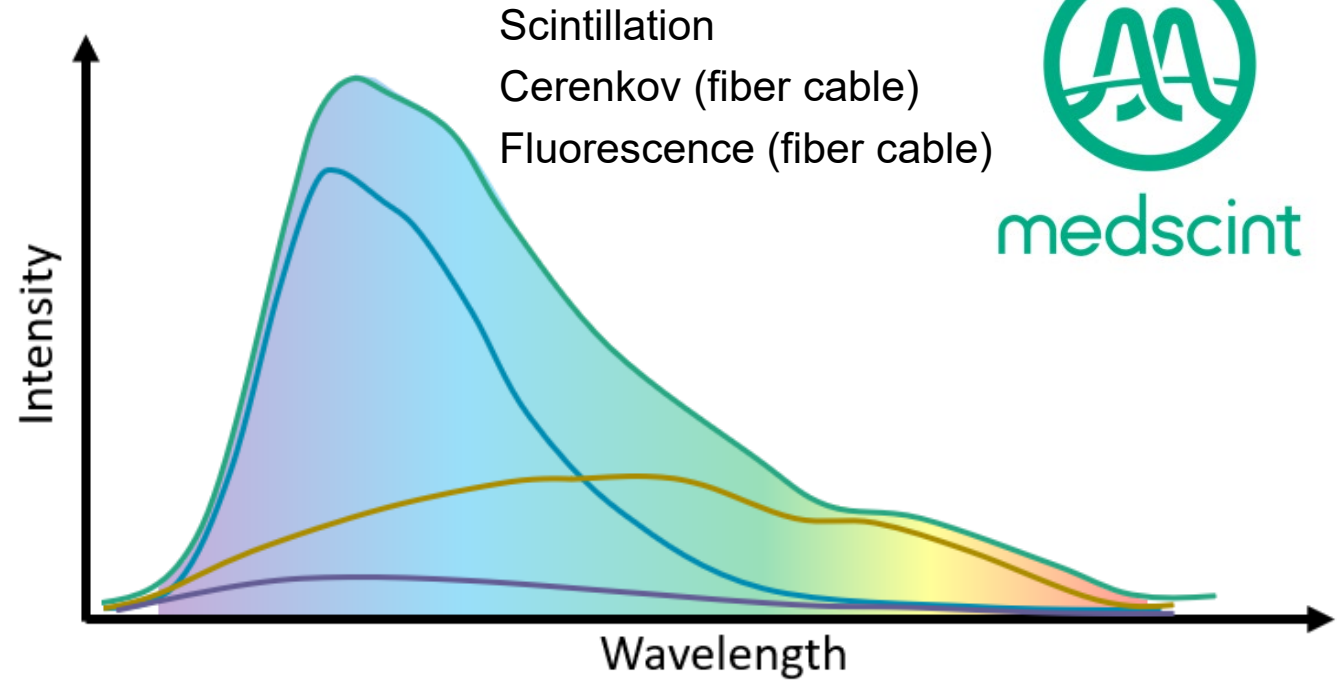
Yoon et al:

Characteristics of the Exradin W1 scintillator in the magnetic field.

Rad. meas. (2019).



HYPERSCINT™ Research Platform



Hyperspectral detection

Complete stem effect removal
Can account for all physical process



Spectral unmixing
of the different
sources of light

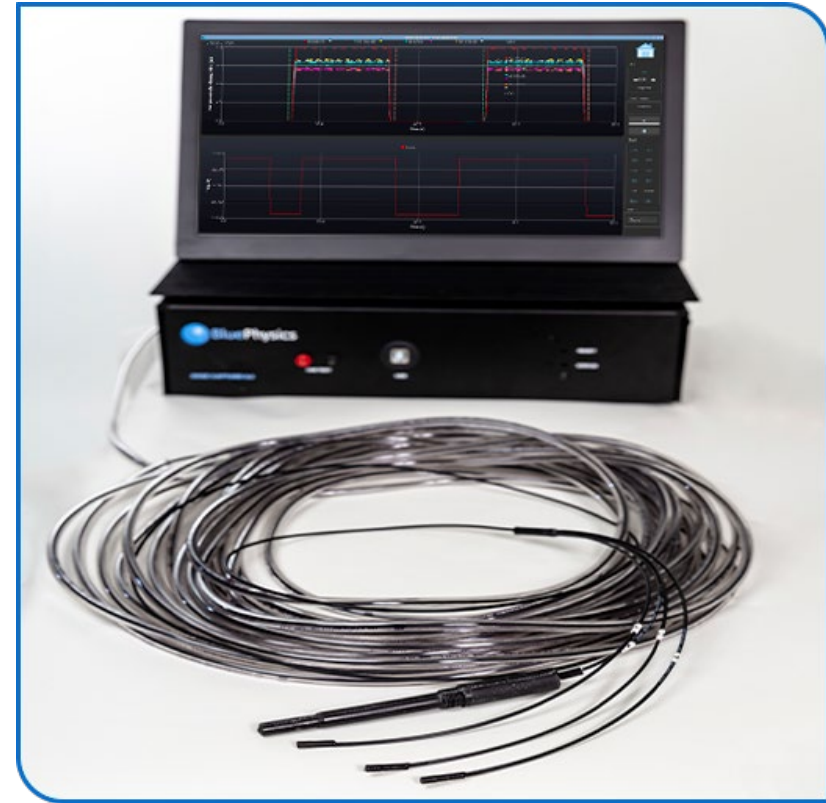
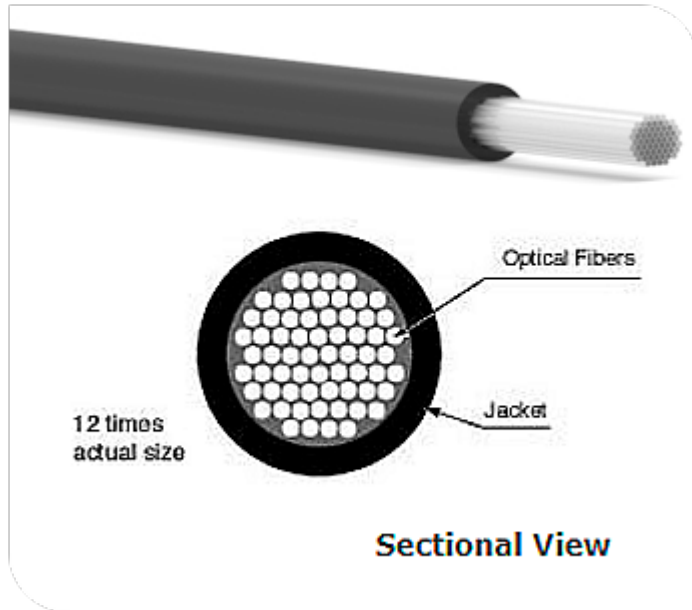
Prescilla Uijtewaal et al. :

Performance of the HYPERSCINT scintillation dosimetry research platform for the 1.5 T MR-linac.

Phys. Med. Biol. (2023).



BluePhysics

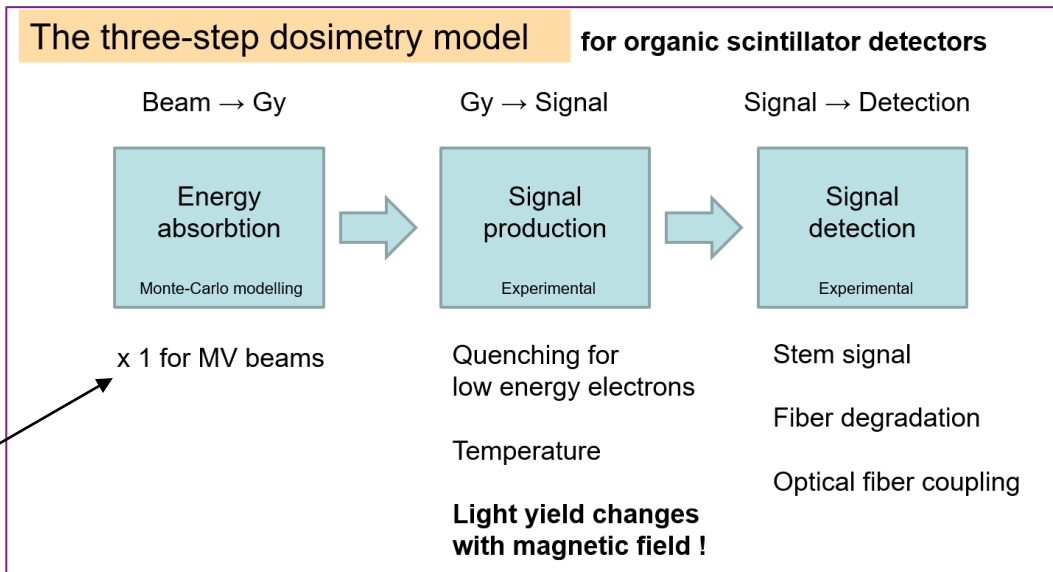
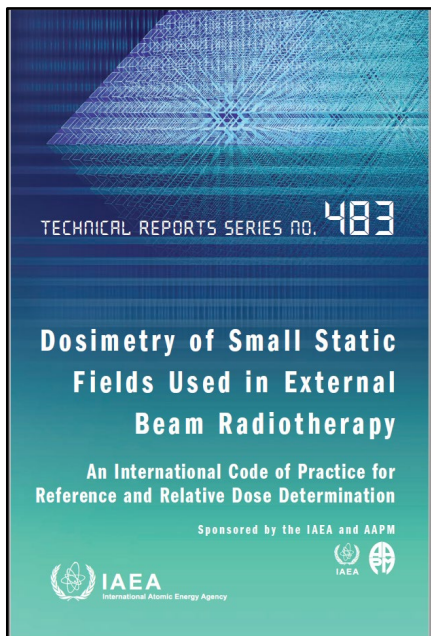


Carlos Ferrer et al.:

Dosimetric characterization of a novel commercial plastic scintillation detector with an MR-Linac.

Medical Phys. (2023).

Performance of scintillators in presence of magnetic fields



- Magnetic field affects the light yield from BCF-60. Important in non-constant B-field situations.
- No change of stem or scintillator spectra thereby supporting the use for the chromatic stem removal technique (both two-channel and based on full spectra information).
- Scintillator measurements support that the field-output factor at the maximum dose point is not significantly changed by the magnetic field.
- Improved uncertainty budget for scintillator based field-output factor measurements.
- Scintillator based field-output factor measurements at five MR linacs.

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