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Monte Carlo simulations of output correction factors in the presence of magnetic field in MRI linacs using Penelope

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Extension of TRS-483 formalism for output factors (OF) in small fields

$$D_{w,Q_{clin}}(S_{eq}) = M_{Q_{clin}}(S_{eq}) \cdot N_{D,w,Q_0} \cdot k_{Q_{msr},Q_0}^{f_{msr},f_{ref}} \cdot k_{Q_{clin},Q_{msr}}^{f_{clin},f_{msr}}(S_{eq})$$

$$D_{w,Q_{msr}}(S_{eq,msr}) = M_{Q_{msr}} \cdot N_{D,w,Q_0} \cdot k_{Q_{msr},Q_0}^{f_{msr},f_{ref}}$$

$$OF(S_{eq}) = \frac{D_{w,Q_{clin}}(S_{eq})}{D_{w,Q_{msr}}(S_{eq,msr})} = ROF(S_{eq}) \cdot k_{Q_{clin},Q_{msr}}^{f_{clin},f_{msr}}(S_{eq})$$

Legend

- Readings
- Calibration coefficient
- k_Q factor
- Output correction factor
- kB factor

$$D_{w,Q_{clin}}(S_{eq}, B) = M_{Q_{clin}}(S_{eq}, B) \cdot N_{D,w,Q_0} \cdot k_{Q_{msr},Q_0}^{f_{msr},f_{ref}} \cdot k_{Q_{clin},Q_{msr}}^{f_{clin},f_{msr}}(S_{eq}) \cdot k_{\vec{B},Q_{clin}}(S_{eq})$$

$$D_{w,Q_{msr}}(S_{eq,msr}, B) = M_{Q_{msr}}(B) \cdot N_{D,w,Q_0} \cdot k_{Q_{msr},Q_0}^{f_{msr},f_{ref}} \cdot k_{\vec{B},Q_{msr}}$$

⋮

$$OF(S_{eq}, B) = \frac{D_{w,Q_{clin}}(S_{eq}, B)}{D_{w,Q_{msr}}(S_{eq,msr}, B)} = ROF(S_{eq}, B) \cdot k_{Q_{clin},Q_{msr}}^{f_{clin},f_{msr}}(S_{eq}) \cdot \frac{k_{\vec{B},Q_{clin}}(S_{eq})}{k_{\vec{B},Q_{msr}}}$$

- Legend**
- Readings
 - Calibration coefficient
 - k_Q factor
 - Output correction factor
 - kB factor

Extension of TRS-483 formalism for output factors (OF) in small fields

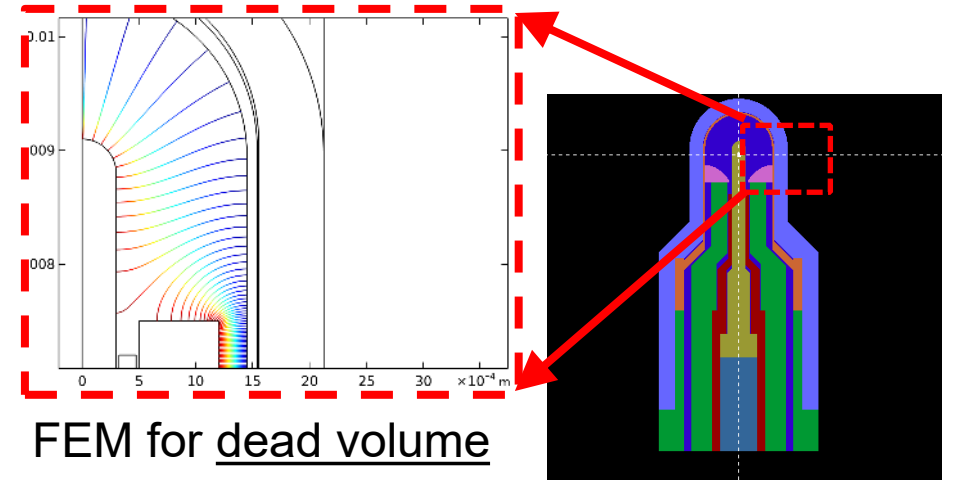
$$k_{Q_{clin}, Q_{msr}}^{f_{clin}, f_{msr}}(S_{eq}, B) = k_{Q_{clin}, Q_{msr}}^{f_{clin}, f_{msr}}(S_{eq}) \cdot \frac{k_{\vec{B}, Q_{clin}}(S_{eq})}{k_{\vec{B}, Q_{msr}}} = k_{Q_{clin}, Q_{msr}}^{f_{clin}, f_{msr}}(S_{eq}) \cdot k_{\vec{B}, Q_{clin}, norm}(S_{eq})$$

TRIS-483
This study

To calculate output correction factors for small field dosimetry in MR-linacs (i.e. with B present) using existing output correction factors determined according to TRS-483 (i.e. without B present)

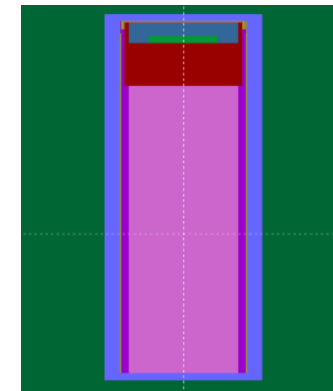
Monte Carlo model for $k_{\vec{B}, Q_{clin, norm}}(S_{eq})$

- PENELOPE 2014 with B-field implemented
- Geometry and materials defined based on manufacturer blueprints
 - Ion chamber PTW 31022
 - Diamond detector PTW 60019
- Sensitive volume is cavity volume – dead volume
- Dead volume determined with Finite Element Method (FEM)
- Phase Space files of Elekta Unity™ MRL for: 0.5, 0.7, 1.0, 1.2, 1.5, 2.0 and 10.0 cm field sides



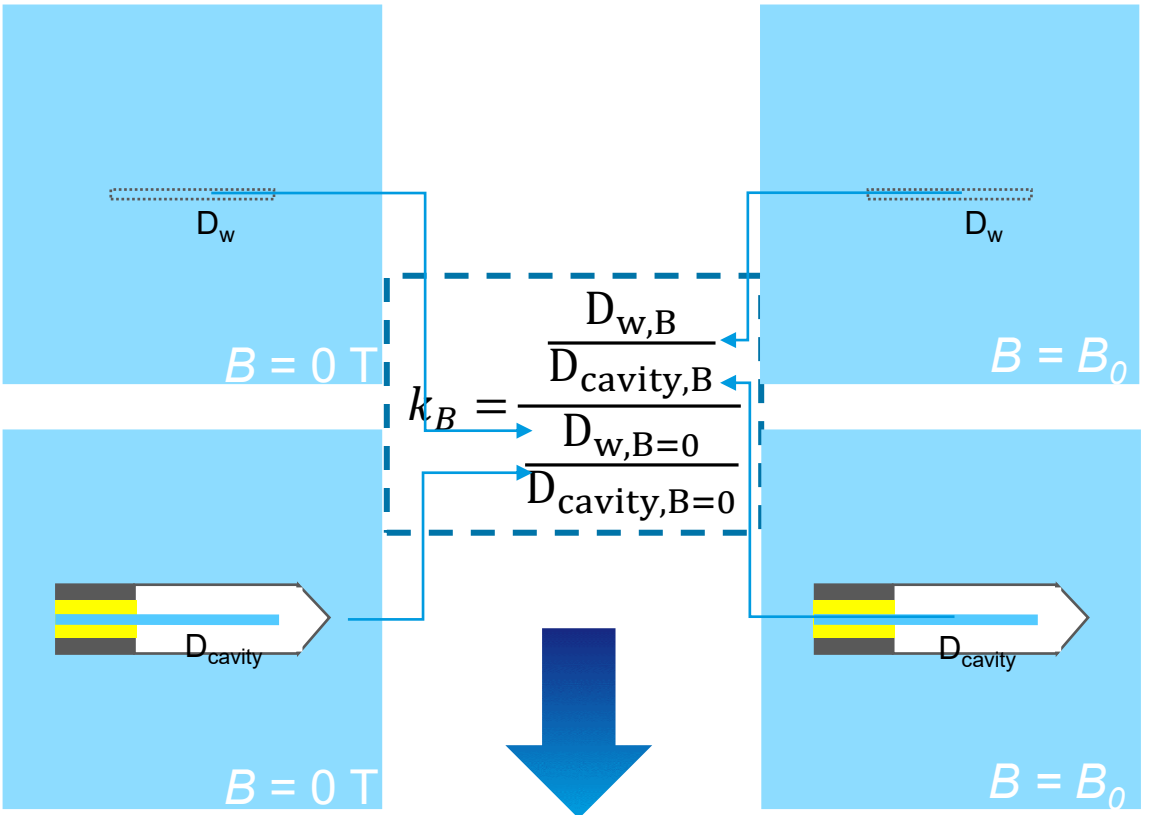
FEM for dead volume

PTW 31022

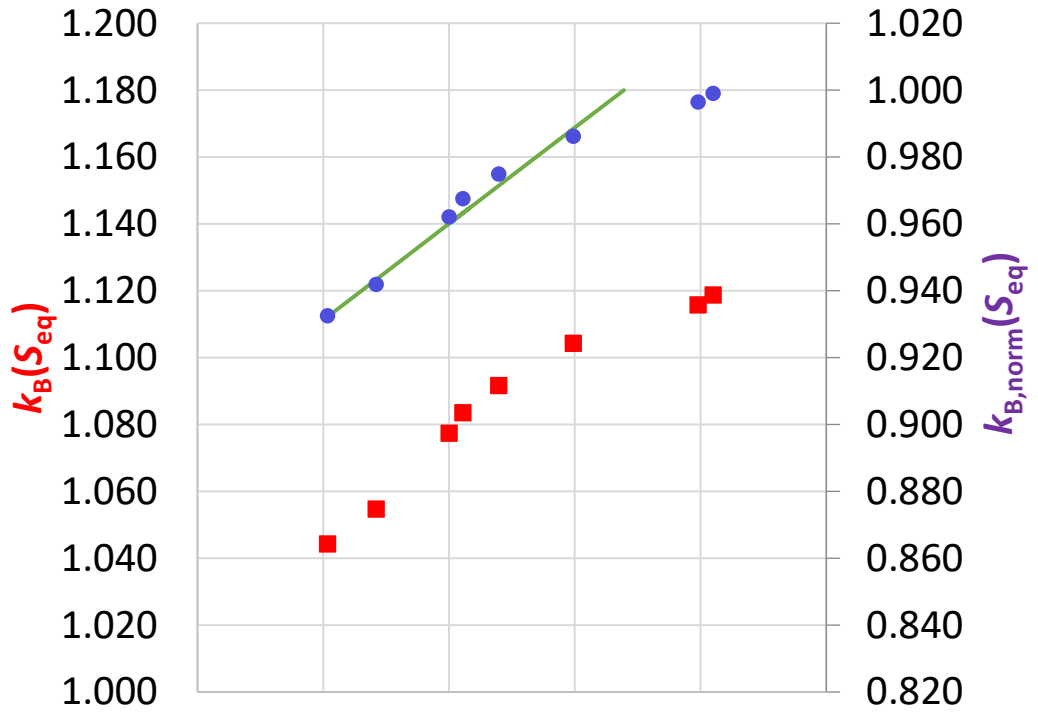


PTW 60019

Simulation and fitting of $k_{\vec{B}, Q_{clin, norm}}(S_{eq})$

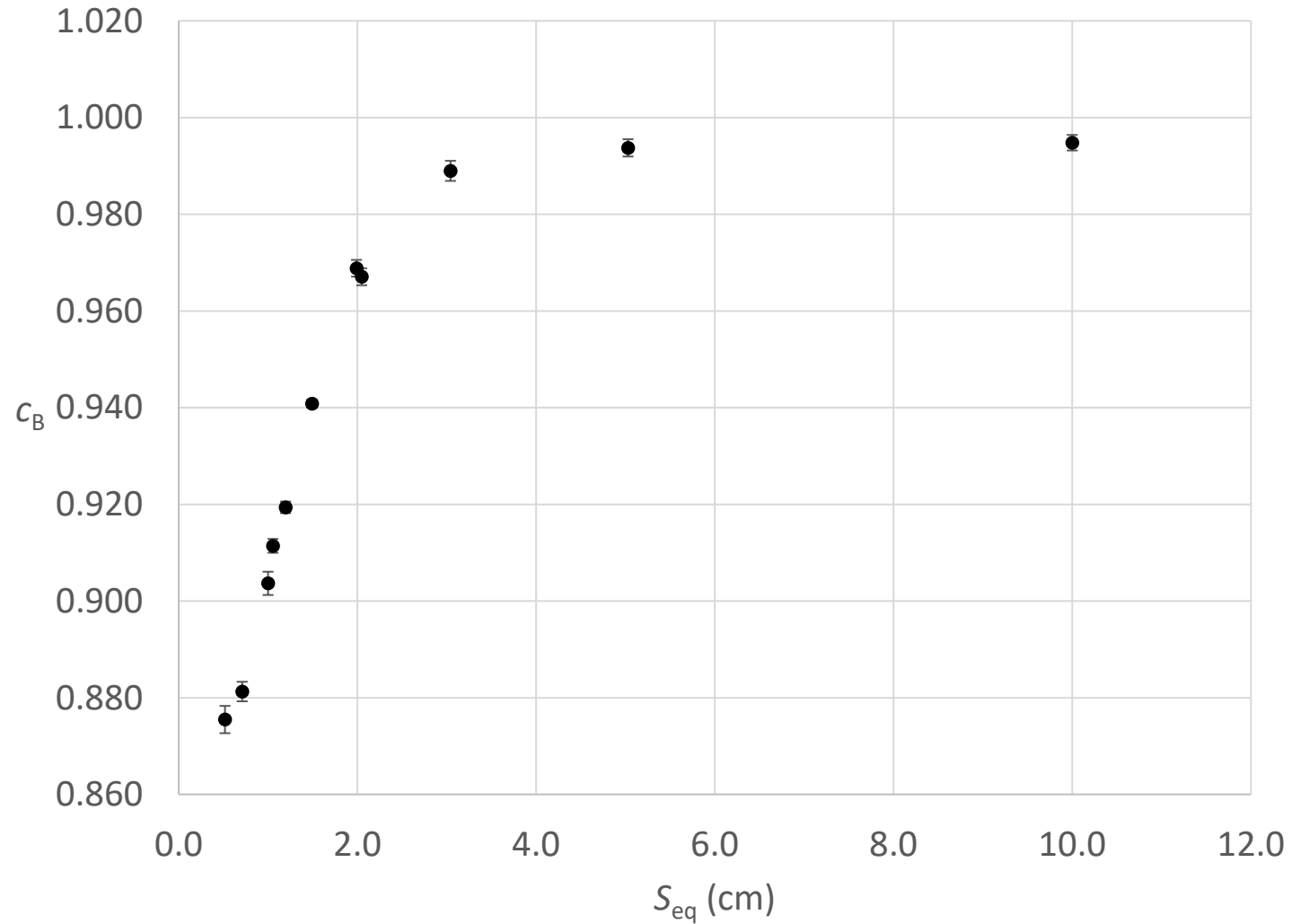


$$\frac{k_{\vec{B}, Q_{clin}}(S_{eq})}{k_{\vec{B}, Q_{msr}}} = \underbrace{\frac{k_{\vec{B}, M, Q_{clin}}(S_{eq})}{k_{\vec{B}, M, 0_{msr}}}}_{\text{Detector dependent}} \underbrace{\frac{c_{\vec{B}}(S_{eq})}{c_{\vec{R}}(msr)}}_{\text{Detector independent}}$$

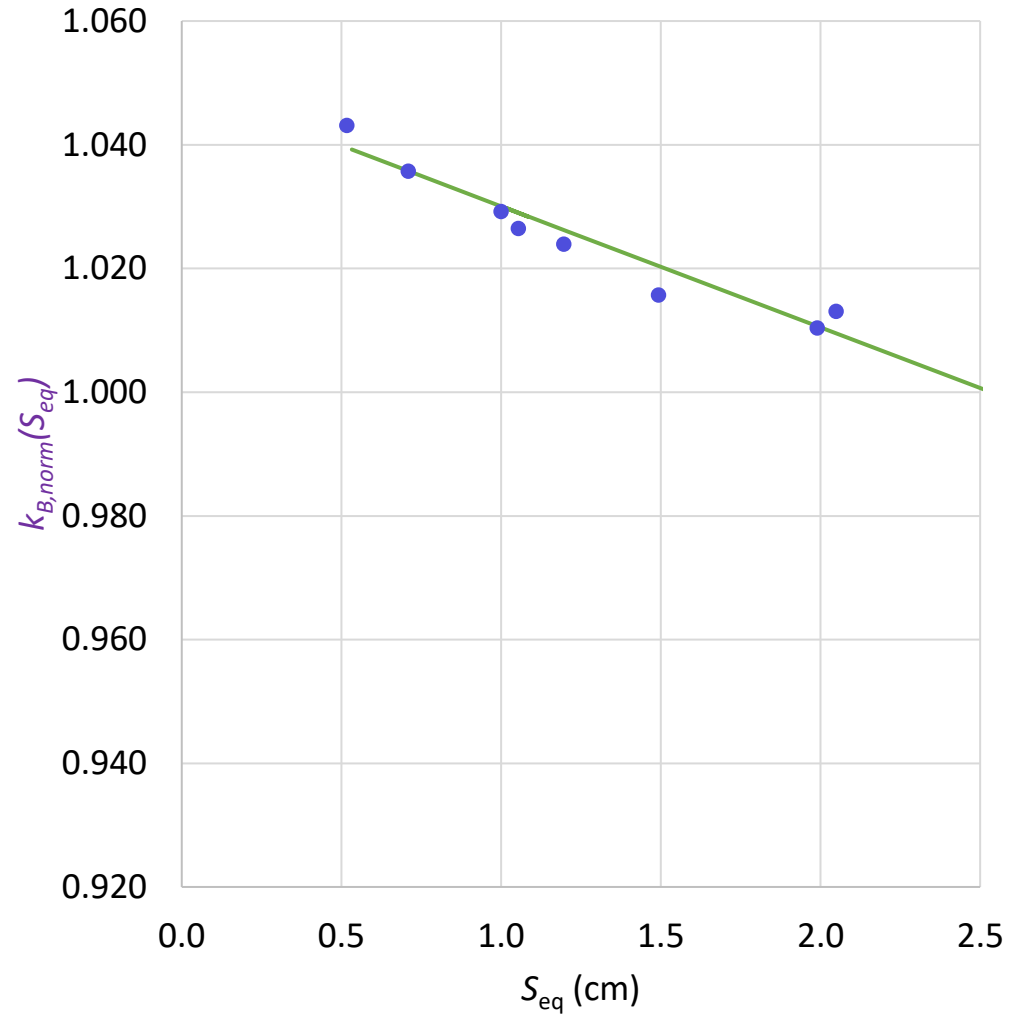


$k_{\vec{B}, Q_{clin, norm}}(S_{eq})$: linear fit below threshold $S_{eq,0}$

$c_{\vec{B}}$ as a function of field size

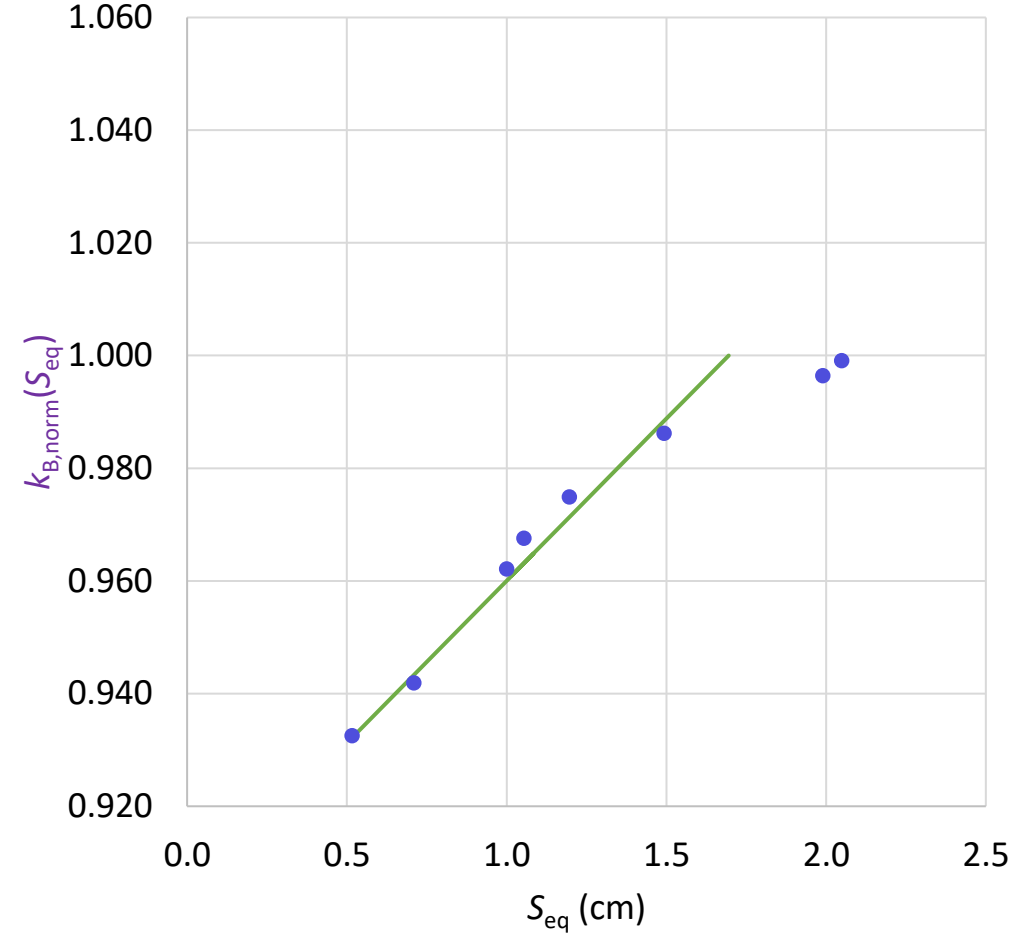


PTW 31022 axial



• $k_{\vec{B},Qclin,norm}(S_{eq})$ — fit

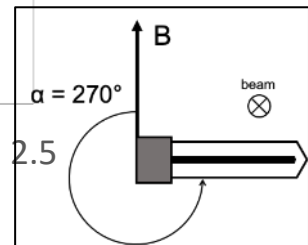
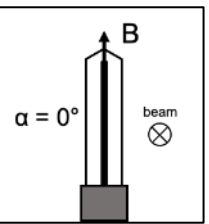
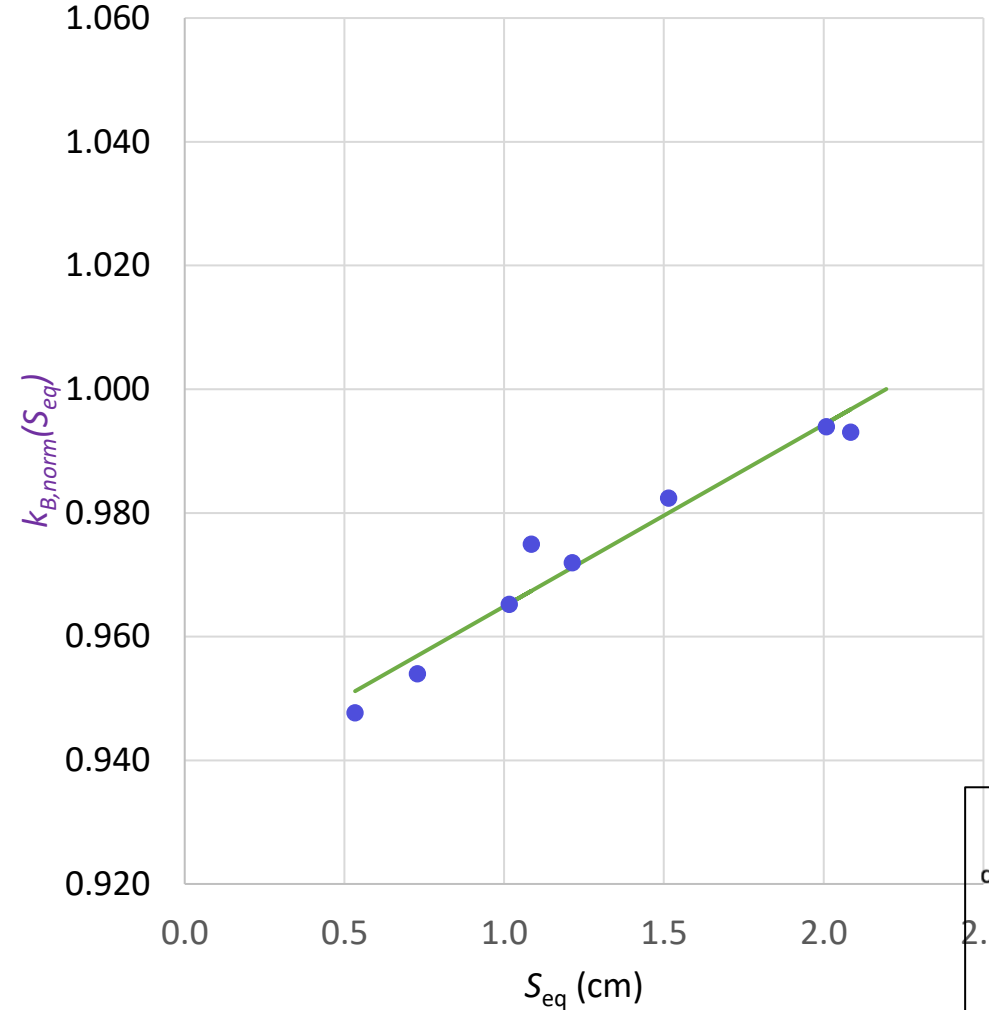
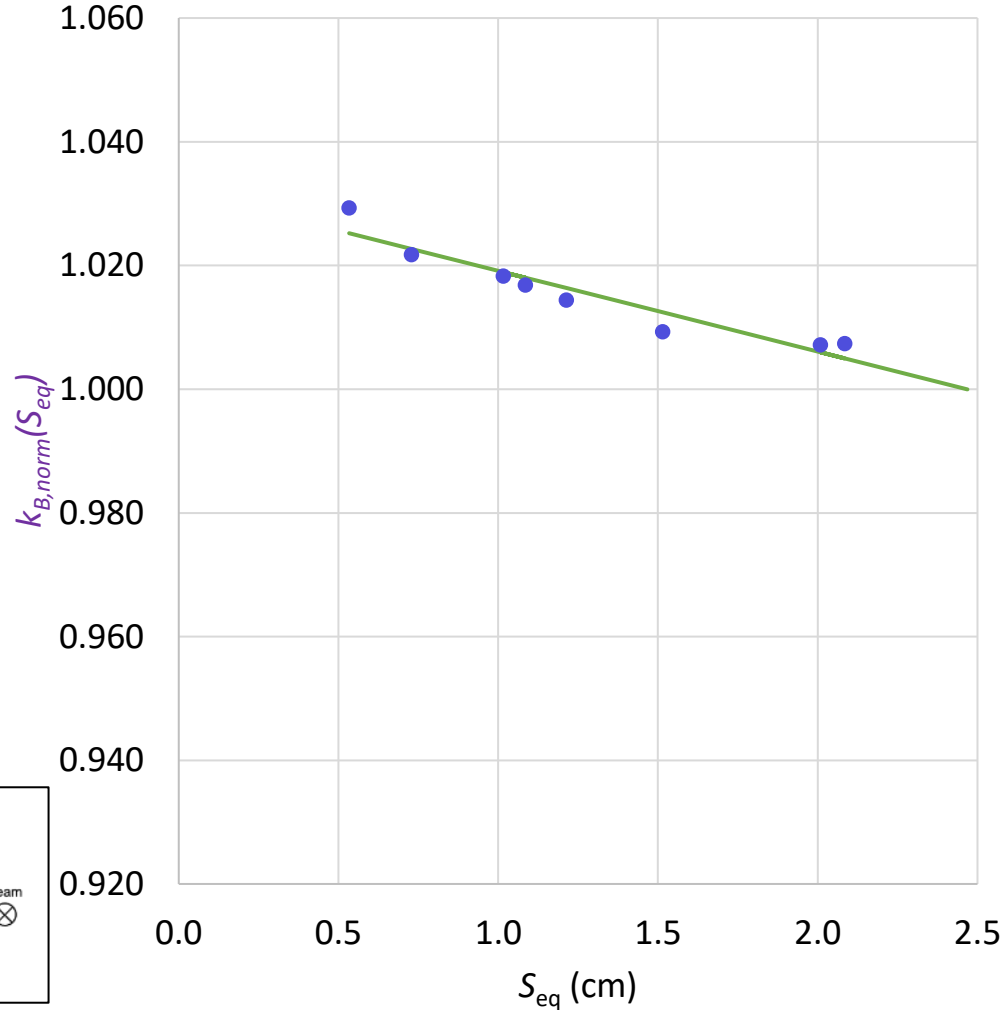
PTW 60019 axial



• $k_{\vec{B},Qclin,norm}(S_{eq})$ — fit

PTW 31022 parallel

PTW 31022 perpendicular



• $k_{\vec{B}, Qclin, norm}(S_{eq})$

— fit

• $k_{\vec{B}, Qclin, norm}(S_{eq})$

— fit

Measurements of output factors (OF) and uncertainty evaluation

- $ROF(S_{eq}, B)$'s measured for MRL Unity:
 - PTW 60019 (axial),
 - PTW 31022 (axial, perpendicular, parallel)

- Nominal square field sizes: 0.5, 0.7, 1.0, 1.2, 1.5, 2.0, 3.0, 4.0, 5.0 and 10.0 cm² => $ROF(S_{eq})$

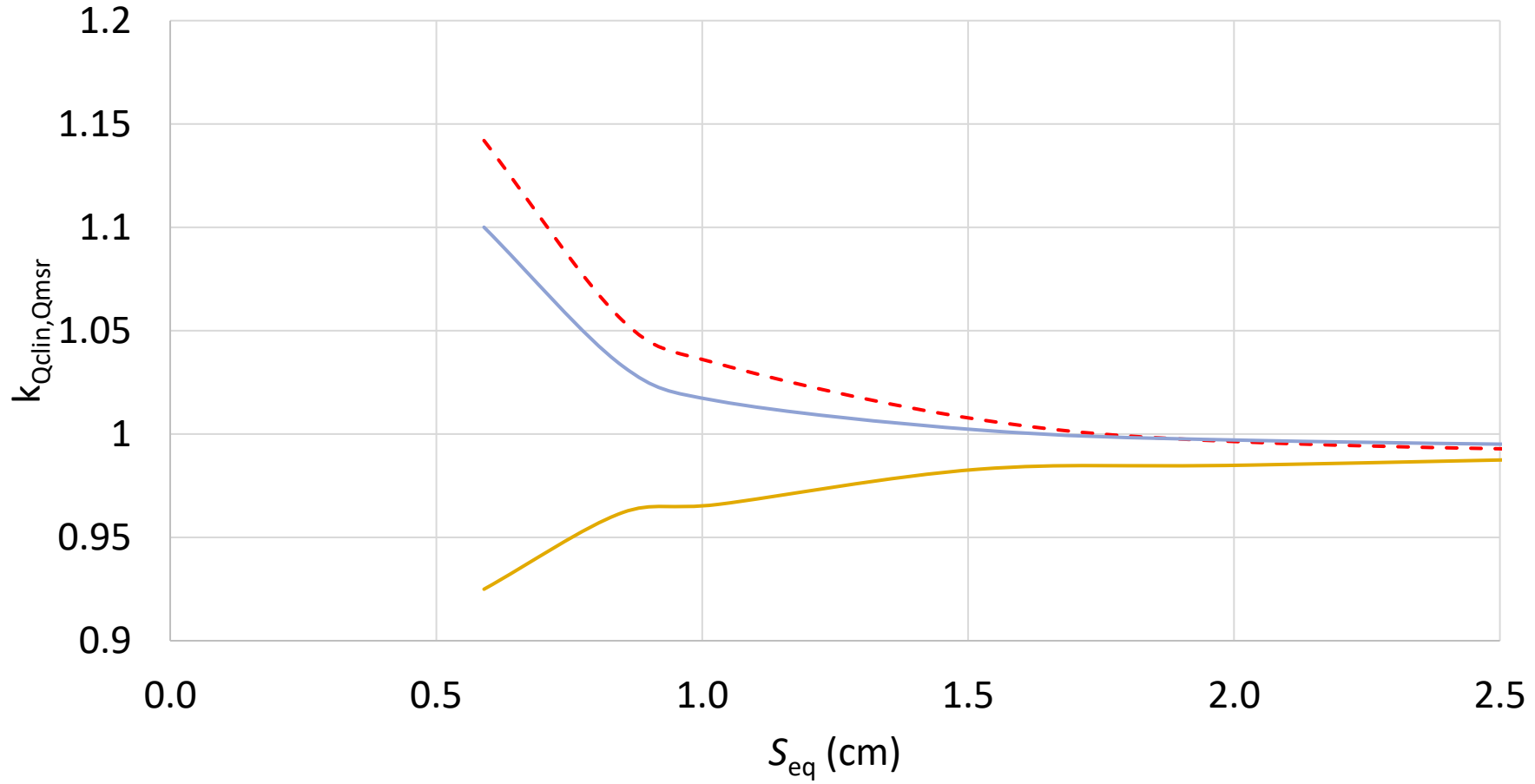
- 3d dose profiles measured with PTW 60019 =>
 - S_{eq} (50% level B =1.5 T profile)
 - $k_{\vec{B}, Q_{clin, norm}}(S_{eq})$ from fit
 - $k_{Q_{clin}, Q_{msr}}^{f_{clin}, f_{msr}}(S_{eq})$ from data of Casar *et al.* Med. Phys (2019, 2020)

- $OF(S_{eq}) = ROF(S_{eq}) \cdot k_{Q_{clin}, Q_{msr}}^{f_{clin}, f_{msr}}(S_{eq}) \cdot k_{\vec{B}, Q_{clin, norm}}(S_{eq})$

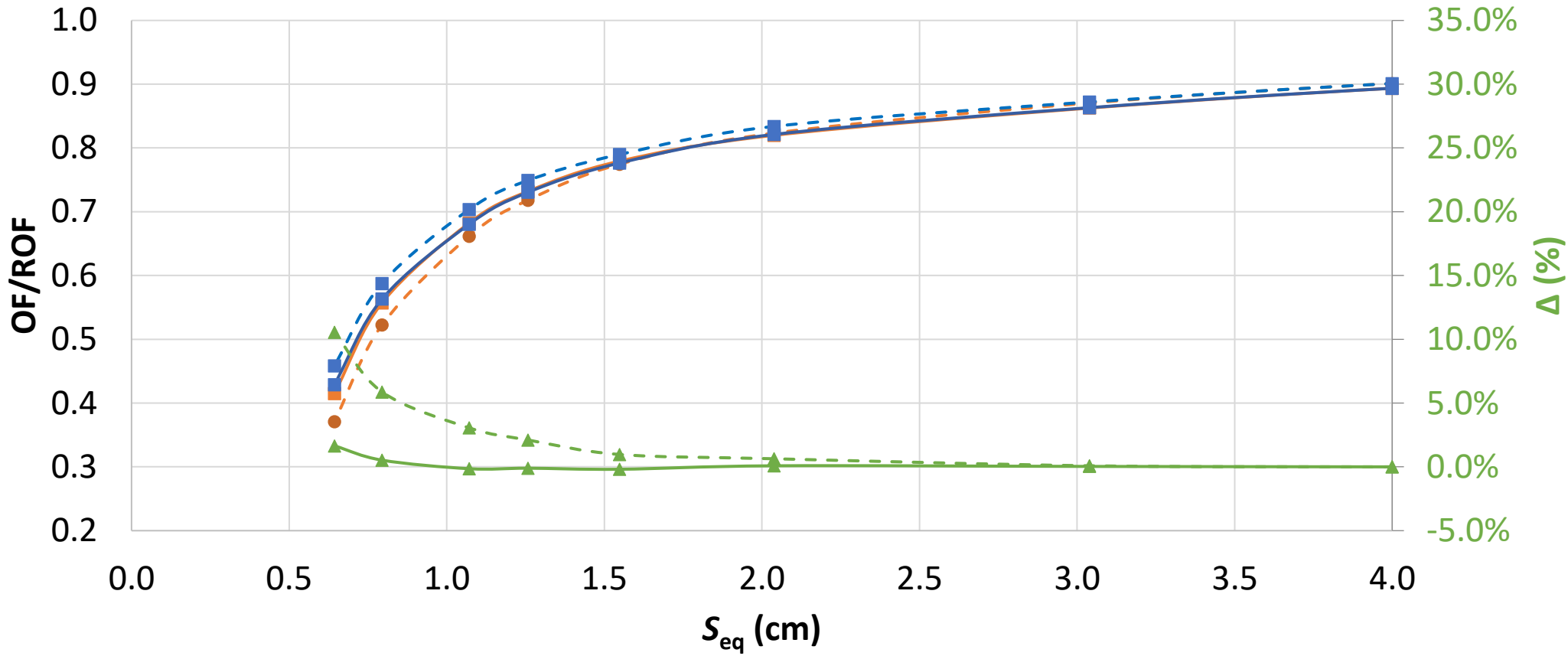
	u_A (%)	u_B (%)
$ROF(S_{eq}, B)$	0.14	0.0 – 1.0
Recombination correction: k_s		0.08
Output correction factor $k_{Q_{clin}, Q_{msr}}^{f_{clin}, f_{msr}}(S_{eq})$ (i.e. B = 0.0 T)		0.8 – 1.8
$k_{\vec{B}, Q_{clin, norm}}(S_{eq})$		0.7 – 0.8
	1.1 – 2.2	

- ### Uncertainty budget
- Uncertainty ROF from positioning and variation in reading
 - Uncertainty output correction factor Casar *et al.* Med. Phys (2019, 2020)
 - Uncertainty $k_{\vec{B}, Q_{clin, norm}}(S_{eq})$ from fit

$k_{Q_{clin}, Q_{msr}}^{f_{clin}, f_{msr}} (S_{eq})$: PTW 31022 and 60019 (Casar *et al.*)



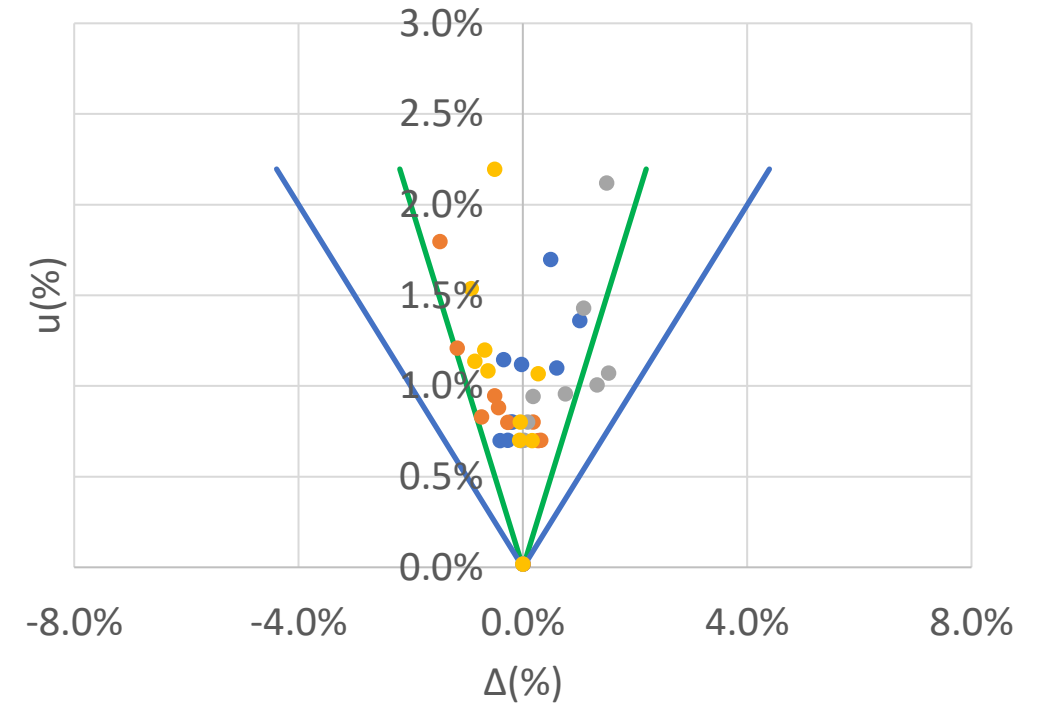
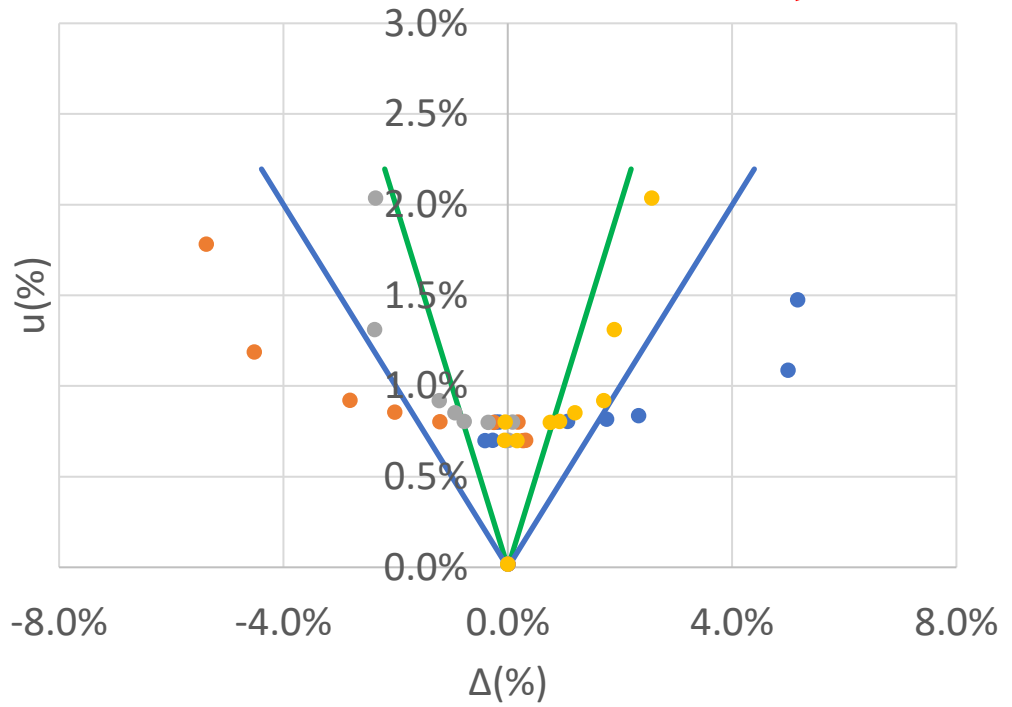
— PTW 60019 mD - 6MV FFF - - - PTW 31022 - 6MV FFF - Radial
— PTW 31022 - 6MV FFF - Axial



-●- ROF - PTW 31022 -■- OF - PTW 31022 -■- ROF - PTW 60019
 -■- OF - PTW 60019 -▲- Δ ROF -▲- Δ OF

$$OF(S_{eq}, B) = ROF(S_{eq}, B) \cdot k_{Q_{clin}, Q_{msr}}^{f_{clin}, f_{msr}}(S_{eq}) \cdot k_{\vec{B}, Q_{clin}, norm}(S_{eq})$$

$$OF(S_{eq}, B) = ROF(S_{eq}, B) \cdot k_{Q_{clin}, Q_{msr}}^{f_{clin}, f_{msr}}(S_{eq}) \cdot k_{\vec{B}, Q_{clin}, norm}(S_{eq})$$



Δ : difference between *OF* and mean *OF* (per field size)
 u : uncertainty on Δ

- *OF* axial – PTW 60019
- *OF* axial – PTW 31022
- *OF* perpendicular – PTW 31022
- *OF* parallel – PTW 31022
- $k = 1$
- $k = 2$

Conclusion

- A method to calculate output correction factors for MR-linacs was developed
- The method is based on existing data for output correction factors for conventional linacs and an additional correction $k_{\vec{B}, Q_{clin, norm}}(S_{eq})$
- $k_{\vec{B}, Q_{clin, norm}}(S_{eq})$ and therefore the output correction factor in magnetic fields strongly depends on detector type and detector orientation
- The validity of the method was demonstrated by the consistency of measured OF data using the simulated $k_{\vec{B}, Q_{clin, norm}}(S_{eq})$ data in combination with the data of Casar *et al. Med. Phys.* (2019, 2020)
- Uncertainty of measured *OFs* using the calculated correction factors is smaller than 2.2 % for field sides 0.5 – 2.0 cm.

Acknowledgement

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